ADAPTIVE STRUCTURED LOW RANK ALGORITHM FOR MR IMAGE RECOVERY

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ABSTRACT

We introduce an adaptive structured low rank algorithm to recover MR images from their undersampled Fourier coefficients. The image is modeled as a combination of a piecewise constant component and a piecewise linear component. The Fourier coefficients of each component satisfy an annihilation relation, which results in a structured Toeplitz matrix. We exploit the low rank property of the matrices to formulate a combined regularized optimization problem, which can be solved efficiently. Numerical experiments indicate that the proposed algorithm provides improved recovery performance over the previously proposed algorithms.

Index Terms— structured low rank matrix, compressed sensing, MRI reconstruction

1. INTRODUCTION

Recovering image data from their noisy partial measurements has been a critical research topic in a wide range of imaging applications including biomedical imaging, remote sensing, and microscopy. The common method is to formulate the image recovery problem as an optimization problem which is the combination of data consistency and regularization term. Conventional regularization penalties include L_1 sparsity or smoothness priors . Recently, structured low rank matrix priors have been introduced as powerful alternatives due to their improvement in image reconstruction quality [1, 2, 3].

Structured low rank matrix algorithms are based on annihilation relationship between the Fourier coefficients of the image and a large set of finite impulse response filter [4, 5]. These algorithms are inspired from the finite-rateof-innovation (FRI) framework [5, 6]. However, the direct extension of FRI model to natural image did not work well. Ongie *et al.* overcome the challenges by presenting an improved signal model based on a class of piecewise smooth functions [3, 7]. This new model lifted the Fourier samples of signals into structured low rank matrix, and the reconstruction of the signal translates to the problem of matrix completion. The annihilation property results in a convolutional structured low rank matrix, which is built from the Fourier coefficients of the image. Researchers have shown that the structured low rank matrix algorithms can provide improved reconstruction performance than standard total variation methods [7, 8].

In this paper, we model an MR image as the combination of a piecewise constant component and a piecewise linear component. For the piecewise constant component, the Fourier coefficients of the gradient of the component satisfy the annihilation relation. We can thus build a structured Toeplitz matrix, which can be proved to be low rank. Similarly, we can obtain a structured low rank matrix from the Fourier coefficients of the second order partial derivatives of the piecewise linear component. By introducing the adaptive method, both the edges and the smooth regions of the image can be accurately recovered. In order to solve the corresponding optimization problem, we adapt the Generic Iteratively Reweighted Annihilating Filter (GIRAF) algorithm proposed in [8], which is based on a half-circulant approximation of the Toeplitz matrix. This algorithm alternates between the estimation of the annihilation filter of the image, and the computation of the image anniihilated by the filter in a least squares formulation. We investigate the performance of the algorithm in the context of compressed sensing MR images reconstruction. Experiments show that the proposed method is capable of providing more accurate recovery results than the state of the art algorithms.

2. BACKGROUND

Consider the general model for a 2-D piecewise smooth image $\rho(\mathbf{r})$ at the spatial location $\mathbf{r} = (x, y) \in \mathbb{Z}^2$:

$$\rho(\mathbf{r}) = \sum_{i=1}^{N} g_i(\mathbf{r}) \chi_{\Omega_i}(\mathbf{r})$$
(1)

where χ_{Ω_i} is a characteristic function of the set Ω_i and the functions $g_i(\mathbf{r})$ are smooth polynomial functions which vanish with a collection of differential operators $\mathbf{D} = \{D_1, ..., D_N\}$ within the region Ω_i . We assume that a bandlimited trigonometric polynomial function $\mu(\mathbf{r})$ vanishes on the edge set $\partial \Omega = \bigcup_{i=1}^N \partial \Omega_i$ of the image:

$$\mu(\mathbf{r}) = \sum_{\mathbf{k}\in\Delta_1} c[\mathbf{k}] e^{j2\pi\langle \mathbf{k}, \mathbf{r} \rangle}$$
(2)

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where $c[\mathbf{k}]$ denotes the Fourier coefficients of μ and Δ_1 is any finite set of \mathbb{Z}^2 . According to [7], the family of functions in (1) is a general form including many common image models by choosing different set of differential operators **D**.

For example, for a piecewise constant image $\rho_1(\mathbf{r})$, the first order partial derivative of the image $\mathbf{D}_1\rho_1 = \nabla \rho_1 = (\partial_x \rho_1, \partial_y \rho_1)$ is annihilated by multiplication with μ in the spatial domain, i.e., $\mu \nabla \rho_1 = 0$. The multiplication in spatial domain translates to the convolution in Fourier domain, by which we can formulate the annihilation property as a matrix multiplication: :

$$\mathcal{T}_{1}(\hat{\rho}_{1})\mathbf{c} = \begin{bmatrix} \mathcal{T}_{x}(\hat{\rho}_{1}) \\ \mathcal{T}_{y}(\hat{\rho}_{1}) \end{bmatrix} \mathbf{c} = \mathbf{0}$$
(3)

where $\mathcal{T}_1(\hat{\rho}_1)$ is a Toeplitz matrix built from the entries of $\hat{\rho}_1$, the Fourier coefficients of ρ_1 . $\mathcal{T}_x(\hat{\rho}_1)$, $\mathcal{T}_y(\hat{\rho}_1)$ are matrices derived from $k_x \hat{\rho}_1[\mathbf{k}]$ and $k_y \hat{\rho}_1[\mathbf{k}]$, omitting the irrelevant factor $j2\pi$. Here **c** is the vectorized version of the filter $c[\mathbf{k}]$, supported in Δ_1 . Consequently, we can obtain:

$$\hat{\rho}_1[\mathbf{k}] * c_1[\mathbf{k}] = 0, \ \mathbf{k} \in \Gamma \tag{4}$$

Here $c_1[\mathbf{k}] = c[\mathbf{k}] * h[\mathbf{k}]$, where $h[\mathbf{k}]$ is any FIR filter. Note that Δ_1 is smaller than Γ , the support of c_1 . Thus, if we take a larger filter size than the minimal filter $c[\mathbf{k}]$, the annihilation matrix will have a larger null space. Therefore, $\mathcal{T}_1(\hat{\rho}_1)$ is a low rank matrix. The method corresponding to this case is referred to as the 1st order structured low rank algorithm for simplicity.

Similarly, for a piecewise linear image ρ_2 , the second order partial derivatives of the image satisfy the annihilation property $\mu^2 \mathbf{D}_2 \rho_2 = 0$, where $\mathbf{D}_2 \rho_2 = (\partial_{xx}^2 \rho_2, \partial_{xy}^2 \rho_2, \partial_{yy}^2 \rho_2)$. Thus the annihilation property in this case can be written in the matrix form as:

$$\mathcal{T}_{2}(\hat{\rho}_{2})\mathbf{d} = \begin{bmatrix} \mathcal{T}_{xx}(\hat{\rho}_{2}) \\ \mathcal{T}_{xy}(\hat{\rho}_{2}) \\ \mathcal{T}_{yy}(\hat{\rho}_{2}) \end{bmatrix} \mathbf{d} = \mathbf{0}$$
(5)

where $\mathcal{T}_{xx}(\hat{\rho}_2)$, $\mathcal{T}_{xy}(\hat{\rho}_2)$, and $\mathcal{T}_{yy}(\hat{\rho}_2)$ are matrices built from $k_x^2 \hat{\rho}_2[\mathbf{k}]$, $k_x k_y \hat{\rho}_2[\mathbf{k}]$, and $k_y^2 \hat{\rho}_2[\mathbf{k}]$, omitting the insignificant factor; **d** is the vector of $d[\mathbf{k}]$, the Fourier coefficients of μ^2 . Here $\mathcal{T}_2(\hat{\rho}_2)$ can also be proved to be a low rank matrix. The method exploiting the low rank property of $\mathcal{T}_2(\hat{\rho}_2)$ is referred to as the 2nd order structured low rank method.

3. ADAPTIVE STRUCTURED LOW RANK IMAGE RECOVERY ALGORITHM

We assume that the recovery of MR images from their undersampled measurements can be modeled as:

$$\mathbf{b} = \mathcal{A}(\hat{\rho}) + \eta \tag{6}$$

where \mathcal{A} is the measurement operator corresponding to Fourier undersampling of $\hat{\rho}$, and η is the zero mean white Gaussian noise.

We are interested in decomposing an MR image ρ into two components $\rho = \rho_1 + \rho_2$, such that ρ_1 represents the piecewise constant component of ρ , while ρ_2 represents the piecewise linear component of ρ . We consider the framework of a combined regularization procedure. Specifically, we attempt to solve the following optimization problem:

$$\{\hat{\rho}_{1}^{\star}, \hat{\rho}_{2}^{\star}\} = \arg\min_{\hat{\rho}_{1}, \hat{\rho}_{2}} \lambda_{1} \|\mathcal{T}_{1}(\hat{\rho}_{1})\|_{p} + \lambda_{2} \|\mathcal{T}_{2}(\hat{\rho}_{2})\|_{p} + \|\mathcal{A}(\hat{\rho}_{1} + \hat{\rho}_{2}) - \mathbf{b}\|^{2}$$
(7)

Here $\mathcal{T}_i(\hat{\rho}_i)$ (i = 1, 2) are the structured Toeplitz matrices in the lifted domain. $\|\cdot\|_p$ is the Schatten p norm (0 , defined for an arbitrary matrix**X** $as <math>\|\mathbf{X}\|_p = \frac{1}{p} \text{Tr}[(\mathbf{X}^*\mathbf{X})^{\frac{p}{2}}] = \frac{1}{p} \sum_i \sigma_i^p$, where σ_i are the singular values of **X**. λ_1 and λ_2 are regularization parameters which balance the data consistency and the degree to which $\mathcal{T}_1(\hat{\rho}_1)$ and $\mathcal{T}_2(\hat{\rho}_2)$ are low rank.

We apply the iterative reweighted least squares (IRLS) algorithm to solve the optimization problem (7). Based on the equation $\|\mathbf{X}\|_p = \|\mathbf{X}\mathbf{H}^{\frac{1}{2}}\|_F^2$, where $\mathbf{H} = (\mathbf{X}^*\mathbf{X})^{\frac{p}{2}-1}$, let $\mathbf{X} = \mathcal{T}_i(\hat{\rho}_i)$ (i = 1, 2), (7) becomes:

$$\{\hat{\rho}_{1}^{\star}, \hat{\rho}_{2}^{\star}\} = \arg\min_{\hat{\rho}_{1}, \hat{\rho}_{2}} \lambda_{1} \|\mathcal{T}_{1}(\hat{\rho}_{1})\mathbf{H}_{1}^{\frac{1}{2}}\|_{F}^{2} + \lambda_{2} \|\mathcal{T}_{2}(\hat{\rho}_{2})\mathbf{H}_{2}^{\frac{1}{2}}\|_{F}^{2} + \|\mathcal{A}(\hat{\rho}_{1} + \hat{\rho}_{2}) - \mathbf{b}\|^{2}$$
(8)

In order to solve (8), we can use an alternating minimization scheme, which alternates between the following subproblems: updating the weight matrices \mathbf{H}_i (i = 1, 2), and solving a weighted least squares problem. Specifically, at *n*th iteration, we compute:

$$\mathbf{H}_{i,n} = \left[\mathcal{T}_i(\hat{\rho}_{i,n})^* \mathcal{T}_i(\hat{\rho}_{i,n}) + \epsilon_n \mathbf{I}\right]^{\frac{p}{2}-1}$$
(9)

$$\{\hat{\rho}_{1,n}, \hat{\rho}_{2,n}\} = \arg\min_{\hat{\rho}_{1}, \hat{\rho}_{2}} \lambda_{1} \|\mathcal{T}_{1}(\hat{\rho}_{1})\mathbf{H}_{1,n}^{\frac{1}{2}}\|_{F}^{2} + \lambda_{2} \|\mathcal{T}_{2}(\hat{\rho}_{2})\mathbf{H}_{2,n}^{\frac{1}{2}}\|_{F}^{2} + \|\mathcal{A}(\hat{\rho}_{1} + \hat{\rho}_{2}) - \mathbf{b}\|^{2}$$
(10)

where $\epsilon_n \rightarrow 0$ is a small factor used to stabilize the inverse. We now show how to efficiently solve the subproblems.

3.1. Update of least squares

First, let $\mathbf{H}_1 = [\mathbf{h}_1^{(1)}, ..., \mathbf{h}_1^{(N)}], \mathbf{H}_2 = [\mathbf{h}_2^{(1)}, ..., \mathbf{h}_2^{(M)}]$, we rewrite the least squares problem (10) as follows:

$$\min_{\hat{\rho}_{1},\hat{\rho}_{2}} \lambda_{1} \sum_{l=1}^{N} \|\mathcal{T}_{1}(\hat{\rho}_{1})\mathbf{h}_{1}^{(l)}\|_{F}^{2} + \lambda_{2} \sum_{m=1}^{M} \|\mathcal{T}_{2}(\hat{\rho}_{2})\mathbf{h}_{2}^{(m)}\|_{F}^{2}
+ \|\mathcal{A}(\hat{\rho}_{1} + \hat{\rho}_{2}) - \mathbf{b}\|^{2}$$
(11)

We now focus on the update of $\hat{\rho}_1$. The update of $\hat{\rho}_2$ can be derived likewise. From the structure property of $\mathcal{T}_1(\hat{\rho}_1)$ and

the convolution relationship, we can obtain:

$$\mathcal{T}_{1}(\hat{\rho}_{1})\mathbf{h}_{1}^{(l)} = \mathcal{P}_{\Gamma_{1}}(\mathbf{M}_{1}\hat{\rho}_{1} * \mathbf{h}_{1}^{(l)}) = \mathcal{P}_{\Gamma_{1}}(\mathbf{h}_{1}^{(l)} * \mathbf{M}_{1}\hat{\rho}_{1})$$
$$= \mathbf{P}\mathbf{C}_{1}^{(l)}\mathbf{M}_{1}\hat{\rho}_{1}, l = 1, ..., N$$
(12)

where $\mathbf{C}_{1}^{(l)}$ denotes the linear convolution by $\mathbf{h}_{1}^{(l)}$, $\mathcal{P}_{\Gamma_{1}}$ is the projection of the convolution to a finite set Γ_{1} of the valid kspace index, which is expressed by the matrix \mathbf{P} . \mathbf{M}_{1} is the linear transformation in k space, which is multiplication by the 1st order Fourier derivatives $j2\pi k_{x}$ and $j2\pi k_{y}$, referred to as the gradient weight lifting case. We can approximate $\mathbf{C}_{1}^{(l)}$ by a circular convolution by $\mathbf{h}_{1}^{(l)}$ on a sufficiently large convolution grid. Then, we can obtain $\mathbf{C}_{1}^{(l)} = \mathbf{FS}_{1}^{(l)}\mathbf{F}^{*}$, where \mathbf{F} is the 2-D DFT and $\mathbf{S}_{1}^{(l)}$ is a diagonal matrix representing multiplication by the inverse DFT of $\mathbf{h}_{1}^{(l)}$. Assuming $\mathbf{P}^{*}\mathbf{P} \approx \mathbf{I}$, we can thus rewrite the first term in (11) as:

$$\lambda_{1} \sum_{l=1}^{N} \|\mathbf{P}\mathbf{C}_{1}^{(l)}\mathbf{M}_{1}\hat{\rho}_{1}\|^{2} = \lambda_{1}\hat{\rho}_{1}^{*}\mathbf{M}_{1}^{*}\mathbf{F}\sum_{\substack{l=1\\\mathbf{S}_{1}}}^{N} \mathbf{S}_{1}^{(l)*}\mathbf{S}_{1}^{(l)} \mathbf{F}^{*}\mathbf{M}_{1}\hat{\rho}_{1}$$
$$= \lambda_{1} \|\mathbf{S}_{1}^{\frac{1}{2}}\mathbf{F}^{*}\mathbf{M}_{1}\hat{\rho}_{1}\|^{2}$$
(13)

where \mathbf{S}_1 is a diagonal matrix with entries $\sum_{l=1}^{N} |\mu_l(\mathbf{r})|^2$, where $\mu_l(\mathbf{r})$ is the trigonometric polynomial of inverse Fourier transform of $\mathbf{h}_1^{(l)}$.

Similarly, the second term in (11) can be rewritten as $\lambda_2 \| \mathbf{S}_2^{\frac{1}{2}} \mathbf{F}^* \mathbf{M}_2 \hat{\rho}_2 \|^2$. Therefore, we can reformulate the optimization problem (11) as:

$$\min_{\hat{\rho}_{1},\hat{\rho}_{2}} \lambda_{1} \| \mathbf{S}_{1}^{\frac{1}{2}} \mathbf{y}_{1} \|_{F}^{2} + \lambda_{2} \| \mathbf{S}_{2}^{\frac{1}{2}} \mathbf{y}_{2} \|_{F}^{2} + \| \mathcal{A}(\hat{\rho}_{1} + \hat{\rho}_{2}) - \mathbf{b} \|^{2}$$
s.t. $\mathbf{F} \mathbf{y}_{1} = \mathbf{M}_{1} \hat{\rho}_{1}, \ \mathbf{F} \mathbf{y}_{2} = \mathbf{M}_{2} \hat{\rho}_{2}$ (14)

The above constrained problem can be efficiently solved using the alternating directions method of multipliers (ADM-M) algorithm [9], which yields to solving the following subproblems:

$$\mathbf{y}_{1}^{(n)} = \min_{\mathbf{y}_{1}} \|\mathbf{S}_{1}^{\frac{1}{2}}\mathbf{y}_{1}\|_{2}^{2} + \gamma_{1}\|\mathbf{q}_{1}^{(n-1)} + \mathbf{F}^{*}\mathbf{M}_{1}\hat{\rho}_{1}^{(n-1)} - \mathbf{y}_{1}\|_{2}^{2}$$
(15)

$$\mathbf{y}_{2}^{(n)} = \min_{\mathbf{y}_{2}} \|\mathbf{S}_{2}^{\frac{1}{2}}\mathbf{y}_{2}\|_{2}^{2} + \gamma_{2}\|\mathbf{q}_{2}^{(n-1)} + \mathbf{F}^{*}\mathbf{M}_{2}\hat{\rho}_{2}^{(n-1)} - \mathbf{y}_{2}\|_{2}^{2}$$
(16)

$$\hat{\rho}_{1}^{(n)} = \min_{\hat{\rho}_{1}} \|\mathcal{A}(\hat{\rho}_{1} + \hat{\rho}_{2}) - \mathbf{b}\|_{2}^{2} + \gamma_{1}\lambda_{1} \|\mathbf{q}_{1}^{(n-1)} + \mathbf{F}^{*}\mathbf{M}_{1}\hat{\rho}_{1} - \mathbf{y}_{1}^{(n)}\|$$
(17)

$$\hat{\rho}_{2}^{(n)} = \min_{\hat{\rho}_{2}} \|\mathcal{A}(\hat{\rho}_{1} + \hat{\rho}_{2}) - \mathbf{b}\|_{2}^{2} + \gamma_{2}\lambda_{2} \|\mathbf{q}_{2}^{(n-1)} + \mathbf{F}^{*}\mathbf{M}_{2}\hat{\rho}_{2} - \mathbf{y}_{2}^{(n)}\|$$
(18)

$$\mathbf{q}_{i}^{(n)} = \mathbf{q}_{i}^{(n-1)} + \mathbf{F}^{*} \mathbf{M}_{i} \hat{\rho}_{i}^{(n-1)} - \mathbf{y}_{i}^{(n)} \quad i = 1, 2$$
(19)

where \mathbf{q}_i (i = 1, 2) represent the vectors of Lagrange multipliers, and γ_i (i = 1, 2) are fixed parameters tuned to improve the conditioning of the subproblems. Subproblems (15) to (18) are quadratic and thus can be solved easily as follows:

$$\mathbf{y}_{1}^{(n)} = (\mathbf{S}_{1} + \gamma_{1}\mathbf{I})^{-1}[\gamma_{1}(\mathbf{q}_{1}^{(n-1)} + \mathbf{F}^{*}\mathbf{M}_{1}\hat{\rho}_{1}^{(n-1)})] \quad (20)$$

$$\mathbf{y}_{2}^{(n)} = (\mathbf{S}_{2} + \gamma_{2}\mathbf{I})^{-1} [\gamma_{2}(\mathbf{q}_{2}^{(n-1)} + \mathbf{F}^{*}\mathbf{M}_{2}\hat{\rho}_{2}^{(n-1)})] \quad (21)$$

$$\hat{\rho}_{1}^{(n)} = (\mathcal{A}^{*}\mathcal{A} + \gamma_{1}\lambda_{1}\mathbf{M}_{1}^{*}\mathbf{M}_{1})^{-1} [\gamma_{1}\lambda_{1}(\mathbf{M}_{1}^{*}\mathbf{F})(\mathbf{y}_{1}^{(n)} - \mathbf{q}_{1}^{(n-1)}) \\ + \mathcal{A}^{*}\mathbf{b} - \mathcal{A}^{*}\mathcal{A}\hat{\rho}_{2}^{(n-1)}] \quad (22)$$

$$\hat{\rho}_{2}^{(n)} = (\mathcal{A}^{*}\mathcal{A} + \gamma_{2}\lambda_{2}\mathbf{M}_{2}^{*}\mathbf{M}_{2})^{-1} [\gamma_{2}\lambda_{2}(\mathbf{M}_{2}^{*}\mathbf{F})(\mathbf{y}_{2}^{(n)} - \mathbf{q}_{2}^{(n-1)}) \\ + \mathcal{A}^{*}\mathbf{b} - \mathcal{A}^{*}\mathcal{A}\hat{\rho}_{1}^{(n-1)}]$$

(23)

3.2. Update of weight matrices

We now show how to update the weight matrices in (9) efficiently based on the GIRAF method [3]. Let $(\mathbf{V}_i, \mathbf{\Lambda}_i)$ denote the eigen-decomposition of $\mathcal{T}_i(\hat{\rho}_i)^* \mathcal{T}_i(\hat{\rho}_i)$ (i = 1, 2), where \mathbf{V}_i is the orthogonal basis of eigenvectors \mathbf{v}_i , and $\mathbf{\Lambda}_i$ is the diagonal matrix of eigenvalues λ_k satisfying $\mathcal{T}_i(\hat{\rho}_i) =$ $\mathbf{V}_i \mathbf{\Lambda}_i \mathbf{V}_i^*$. Then we can rewrite the weight matrices \mathbf{H}_1 and \mathbf{H}_2 as:

$$\begin{aligned} \mathbf{H}_{i} &= \left[\mathbf{V}_{i}(\mathbf{\Lambda}_{i} + \epsilon \mathbf{I})\mathbf{V}_{i}^{*}\right]^{\frac{p}{2}-1} = \mathbf{V}_{i}(\mathbf{\Lambda}_{i} + \epsilon \mathbf{I})^{\frac{p}{2}-1}\mathbf{V}_{i}^{*}, \ i = 1, 2 \end{aligned} (24) \end{aligned}$$
Thus, one choice of the matrix square root $\mathbf{H}_{i}^{\frac{1}{2}}$ is $(\mathbf{\Lambda}_{i} + \epsilon \mathbf{I})^{\frac{p}{4}-\frac{1}{2}}\mathbf{V}_{i}^{*}.$

4. RESULTS

The performance of the proposed method is investigated in the context of compressed sensing MR images reconstruction. In the experiments, we assume that the measurements are acquired using variable density random retrospective sampling pattern under different acceleration factors. For each A operator, we determine the regularization parameters to obtain the optimized signal-to-noise ratio (SNR) to ensure fair comparisons between different methods.

We first study the performance of the proposed method $_2$ for the recovery of a piecewise smooth phantom image from 2 its noiseless k-space data at 4-fold undersampling in Fig. 1. Note that the decomposition results by the propose method indicated in (c) and (d) clearly show the piecewise constant $_2$ component ρ_1 and the piecewise linear component ρ_2 of the 2 image. We observe that the proposed method provides lower errors compared with the standard TV, the 1st and 2nd order

structured low rank methods, and the total generalized variation (TGV) method [10]. The computational time with the GPU implementation for the 1st order method, the proposed method, and TGV were 9.4 sec, 18.3 sec, and 5.2 sec, respectively.



Fig. 1: Recovery of a piecewise smooth phantom image from the 4-fold undersampled measurements using 15×15 filter size. (a)-(b): The actual and the zoomed version of the image. (c)-(d): The decomposition results. (e): The sampling mask. (f)-(j): Reconstructions using the proposed method, the 1st and 2nd order method, TV, and TGV, respectively. (k)-(o): Error images.

In Fig. 2, we demonstrate the performance of the proposed approach on the reconstruction of a brain MR image from 5-fold undersampling. The results show that TV leads to patchy recovered image. While the proposed method outperforms the other schemes in providing more accurate recovered image. In Fig. 3, we demonstrate the effect of the proposed scheme using different filter sizes on the recovery of another brain MR image data at acceleration factor of 2. We observe that as the filter size increases, the proposed method provides better result, indicating the benefits of using larger filters.



Fig. 2: Recovery of the brain MR dataset from 5-fold undersampled measurements using 15×15 filter size. (a)-(b): The actual and the zoomed version of the original image. (c)-(d): The decomposition results. (e)-(h): Reconstructions using the proposed method, the 1st and 2nd order method, and standard TV, respectively. (i)-(l): Error images.



(f) Sampling mask (g) Error of 1st (h) Error of proposed (i) Error of proposed (j) Error of TGV

Fig. 3: Recovery of the brain MR dataset from 2-fold undersampled measurements. (a): The actual zoomed image. (b): The recovery image using the 1st order scheme with filter size of 15×15 . (c)-(d): The reconstructions using the proposed method with filter size of 15×15 and 31×31 , respectively. (e): The reconstruction of TGV. (f): The undersampling pattern. (g)-(j): Error images.

5. CONCLUSION

We proposed a novel adaptive structured low rank algorithm to recover MR images from their undersampled k space measurements, by the assumption that an MR image can be modeled as the combination of a piecewise constant component and a piecewise linear component. Experiments show that the proposed algorithm provides more accurate recovery results compared with the state of the art approaches.

6. REFERENCES

- K. H. Jin, D. Lee, and J. C. Ye, "A general framework for compressed sensing and parallel MRI using annihilating filter based low-rank Hankel matrix," *IEEE Transactions on Computational Imaging*, vol. 2, no. 4, pp. 480–495, 2016.
- [2] J. P. Haldar, "Low-rank modeling of local k-space neighborhoods (LO-RAKS) for constrained MRI," *IEEE Transactions on Medical Imaging*, vol. 33, no. 3, pp. 668–681, 2014.
- [3] G. Ongie and M. Jacob, "Off-the-grid recovery of piecewise constant images from few Fourier samples," *SIAM Journal on Imaging Sciences*, vol. 9, no. 3, pp. 1004–1041, 2016.
- [4] H. Pan, T. Blu, and P. L. Dragotti, "Sampling curves with finite rate of innovation," *IEEE Transactions on Signal Processing*, vol. 62, no. 2, pp. 458–471, 2014.
- [5] M. Vetterli, P. Marziliano, and T. Blu, "Sampling signals with finite rate of innovation," *IEEE Transactions on Signal Processing*, vol. 50, no. 6, pp. 1417–1428, 2002.
- [6] I. Maravic and M. Vetterli, "Sampling and reconstruction of signals with finite rate of innovation in the presence of noise," *IEEE Transactions on Signal Processing*, vol. 53, no. 8, pp. 2788–2805, 2005.
- [7] G. Ongie and M. Jacob, "Recovery of piecewise smooth images from few Fourier samples," in *Sampling Theory and Applications (SampTA)*, 2015 International Conference on. IEEE, 2015, pp. 543–547.
- [8] G. Ongie and M. Jacob, "A fast algorithm for structured low-rank matrix recovery with applications to undersampled MRI reconstruction," in *Biomedical Imaging (ISBI), 2016 IEEE 13th International Sympo*sium on. IEEE, 2016, pp. 522–525.
- [9] E. Esser, "Applications of Lagrangian-based alternating direction methods and connections to split Bregman," *CAM report*, vol. 9, pp. 31, 2009.
- [10] Florian Knoll, Kristian Bredies, Thomas Pock, and Rudolf Stollberger, "Second order total generalized variation (TGV) for MRI," *Magnetic resonance in medicine*, vol. 65, no. 2, pp. 480–491, 2011.